

On bioheat equation and its modifications

Nataliya Kizilova, *Kharkov, Ukraine*

Anatoliy Korobov, *Kharkov, Ukraine*

Mathematical modeling of the optical and infrared heating of biological tissues is based on the Pennes bioheat balance equation [1] and its modifications, the single-phase lag (SFL) [2] and dual-phase lag (DFL) [3] models. The Pennes bioheat equation is

$$\rho c \frac{\partial T}{\partial t} = \operatorname{div}(k \nabla T) + q_{met} = q_h + \rho_b c_b w_b (T_b - T), \quad (1)$$

where T is the temperature, ρ, c, k are the density, specific heat and thermal conductivity of the tissue, the subscript b relates to the blood, w_b is the blood perfusion rate, q_{met} and q_h are metabolic and photostimulated heats.

The SFL model accounts for the time delay τ_q between the heat flux q and the temperature gradient ∇T that give the equation

$$\rho c \tau_q \frac{\partial^2 T}{\partial t^2} + (\rho c + \rho_b c_b w_b \tau_q) \frac{\partial T}{\partial t} = \operatorname{div}(k \nabla T) + q_{met} + q_h + \rho_b c_b w_b T_b. \quad (2)$$

The DTL model accounts for two time lags τ_q and τ_T and has the form similar to (2). As it was shown, the SFL and DFL models are thermodynamically inconsistent, while the Guyer-Krumhansl equation as an example of the non-Fourier heat conduction law is thermodynamically correct.

In this paper the 1D solutions of the models (1)-(2) and the Guyer-Krumhansl equation for the surface heating of human skin are considered. The computational results are compared to the measured curves $T(t)$. It is shown, the Guyer-Krumhansl equation gives the best correspondance between the computational and measured curves for both heating and relaxation precesses.

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